Patients were informed about the examination and also for breath holding. Imaging performed with Bolus tracking program. After scenogram, single slice is taken at the level of pulmonary truncus. A bolus tracking is placed at pulmonary truncus and trigger is adjusted to 100 HU (Hounsfield Unit), 70ml nonionic contrast agent at the rate of 4mL/sec with an automated syringe (Optistat Contrast Delivery System, Liebel-Flarsheim, USA) is used. When opacification is reached at the pre-adjusted level exam performed from the supraclavicular region to the diaphragms. Contrast injection performed via 18-20G intra venous cannula that was placed at antecubital vein. Scanning parameters were 120 kV, 80-120 mA, slice thickness 1 mm, pitch 1.0-1.2. Images reconstructed with 1mm and 5mm thickness, and evaluated at mediastinal window (WW 300, WL 50) with advanced workstation (Wizard, Siemens, AG, Erlanger, Germany) in coronal sagittal and axial planes. Oblique plans used if needed. Each exam consists of 400-500 images with 512x512 resolutions.

II. MATERIALS AND METHODS

A. Data Retrieval

In this study, data was collected from Dr. Siyami Ersek thoracic and cardiovascular surgery training and research hospital. All pulmonary computed tomographic angiography exams performed with 16 detectors CT (Somatom Sensation 16, Siemens, AG, Erlanger, Germany) equipment.

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CTA images, which are in hands, are 300 as being 2D. Firstly, to segment lung, each image has been threshold using images $>-200$ HU as the level of threshold. Each of components in the image has been labeled with “Connected Component Labeling algorithm” (CCL) as 2D and ones whose number of voxels are under 500 were removed from the image. Lastly, regions, outside of patient’s body were removed and regions, inside of patient’s body were determined as right and left lungs [16]. After lung segmentation, MR was determined. For this, in each slice, minimum and maximum points of lung region were detected and, $X_{min}$, $X_{max}$, $Y_{min}$, and $Y_{max}$ values were integrated. These values indicate the corner of the rectangle border (Fig 2b). Mediastinum region was determined as a rectangle which was reduced 20 voxels inward from each side of the rectangle border of lung region (Fig 2c).

In Figure 4, the component, shown with number 1, is AscA. The component, shown with number 2 is DesA. This image is the first image which is processed and which truncus rises. AscA is the component at the top of the image, DesA is the component which is the nearest to right side of the image in first image which truncus rise belongs to the all patients.

To segment AscA and DesA, firstly $X_{min}$ and $Y_{max}$ points are determined in Fig.4. Then, components in the image have been labeled with CCL as 2D and the labels which have $X_{min}$ and $Y_{max}$ points are detected. Component which has label in $X_{min}$ point is detected as 2D AscA. Others are removed (Fig. 5a). Component which has label in $Y_{max}$ point is detected as 2D DesA. Others are removed (Fig. 5b).

After these processes, each image has been threshold using $150$ HU < Image < $500$ HU as the level of threshold (Fig 3).

Then, components which are outside of the MR were removed from the 2D images and the small gaps on the components were filled by gap filling filters. The small objects in lung region are problem. To remove the small objects, each component in the image has been labeled with CCL as 2D and ones whose number of voxels is under 250 were removed from the image (Fig. 4). These processes have been applied to all of the images from the image beginning of truncus to the image end of pulmonary vein.

AscA which carried out at the end of gathering is seen in white color because of its value of 2 and other components are seen in grey color because of their value of 1 (Fig. 6a). In the same way, DesA which carried out at the end of gathering is seen in white color because of its value of 2 and other components are seen in grey color because of their value of 1 (Fig. 6b). Components which have value of 1 are removed from both of the images. Thence AscA and DesA are detected in the all images as 2D. All of the 2D images are formed 3D AscA and DesA images.

### III. Conclusion and Discussion

The method, which has been tried at this work, applied to 30 different patients. Because of the fact that the segmentation in all CTA images (approximately 300) belonging to one
patient is solved in a short time as 1-2 minutes, it has a fast working property. It has been seen that the results at the end of applied method adjust to AscA and DesA determined with hand by the radiologists. With the help of this work, which performs AscA and DesA in a fast way, detection of aortic plaques, aneurysms, calcification, or stenosis can be done in a faster way.

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